

## EDITORIAL COMMENT

# T<sub>1</sub> Mapping for Diffuse Myocardial Fibrosis

## A Key Biomarker in Cardiac Disease?\*

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Multicellular organisms are built of cells embedded in the interstitium, the scaffolding of organs and tissues. In disease, the ratio between cells and interstitium changes due to interstitial expansion as a result of increased collagen (focal and diffuse fibrosis) or accumulation of exogenous material such as amyloid. In most organs and diseases (e.g., liver cirrhosis), diffuse fibrosis plays a key role, and fibrosis quantification guides therapy. In the heart, diffuse fibrosis appears histologically ubiquitous, but it remains clinically invisible, and the gold standard test, invasive myocardial biopsy, has significant morbidity and sampling error. Cardiovascular

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magnetic resonance measures focal fibrosis (scar) by using late gadolinium enhancement, but this method is unable to quantify diffuse fibrosis. T<sub>1</sub> mapping, a new cardiovascular magnetic resonance technique, can now noninvasively quantify the myocardial extracellular volume (ECV), reflecting diffuse fibrosis (1).

The longitudinal relaxation time (T<sub>1</sub>) of a tissue indicates how rapidly protons recover after a radiofrequency pulse. Pre-contrast (native) T<sub>1</sub> varies with water content and may increase in cases of diffuse myocardial fibrosis (2), but it inherently embodies composite signal from both cells and interstitium, and it varies with measurement technique and

magnetic resonance imaging field strength. After extracellular gadolinium-based contrast administration, T<sub>1</sub> is dominated by and is inversely proportional to the concentration of gadolinium. Measuring T<sub>1</sub> after contrast provides a value linked to the interstitium, but post-contrast T<sub>1</sub> also varies due to gadolinium dose, clearance rate, time post bolus, body composition, and hematocrit. If the change in T<sub>1</sub> pre-contrast and post-contrast is measured in both blood and myocardium after equilibration of the contrast distribution, the partition coefficient can be calculated. By correcting for the hematocrit level, the myocardial ECV is derived, which is a more stable and biologically significant biomarker. The utility of ECV measurement is increasingly being reported across the spectrum of cardiology (3), and new data show ECV, in unselected patients, predicts outcomes at least as strongly as left ventricular ejection fraction (4,5).

In this issue of the *Journal*, Liu et al. (6) present a large cohort, based on CMR data from 1,231 participants aged 54 to 93 years from the Multi-Ethnic Study of Atherosclerosis (MESA) study, and investigated the relationship between CMR indices and age/sex. The authors are congratulated for integrating T<sub>1</sub> measurement into the MESA study, providing data on normal ranges, mechanisms of sex differences, and correlations with clinical findings from this well-characterized cohort. Previously, only small, single-center studies have demonstrated a correlation between ECV and age (3). The authors used a single breath-hold Modified Look-Locker Inversion recovery (MOLLI) (7) sequence in one mid short axis slice, showing that women had significantly higher pre-contrast T<sub>1</sub> times and partition coefficient as well as lower post-contrast T<sub>1</sub> times than men. When hematocrit data were available, ECV was higher in women than in men (28.1 ± 2.8% vs. 25.8 ± 2.9%; p < 0.001). Using multivariable linear regression, ECV increased with age in men with every decade (p < 0.001), but in women, ECV decreased with age. In the overall cohort, ECV was correlated with age (R<sup>2</sup> = 0.021; p = 0.012).

What are we to make of these results? At face value, they may explain some sex differences in the prevalence of congestive heart failure (8) and support the idea that diffuse myocardial fibrosis increases with age. However, unresolved questions remain. Age and ECV correlated weakly, with an R<sup>2</sup> of only 0.021, meaning that 97.9% of all ECV variation is explained by factors other than age. Although the age-ECV relation was statistically significant, the clinical significance is less certain. In fact, one could reasonably conclude, that because age is so minimally related to myocardial fibrosis, most people can age successfully without inexorable, age-related myocardial fibrosis—an optimistic interpretation indeed. Second, risk adjustment addressed the presence of comorbidities but not their severity. Disease severity, including longer “exposure” to comorbidity (e.g., hypertension), may increase with age and introduce residual confounding not addressed by the statistical modeling. Third, the sex-related results may be confounded by menopause.

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From a technical perspective, the T<sub>1</sub> mapping field is rapidly advancing. The iteration of the Modified Look-Locker Inversion recovery (MOLLI) sequence used in this study (6) has improved. Single breath-hold mapping (in which each pixel carries the T<sub>1</sub> value) has replaced multi-breath-hold methods, and newer refinements include iterative reconstruction, shorter breath-holds, better sequence design, and, lately, ECV maps with pixel-by-pixel representation of ECV for a simplified detection, measurement and quantitative display of diffuse fibrosis (9). There is an apparent spectrum of interstitial expansion with cardiac amyloid, aortic stenosis, and cardiomyopathy having large changes in ECV; age and sex, however, have much smaller or possibly no contributions (10). The ratio of pathophysiological signal to measurement error determines test performance. T<sub>1</sub> mapping seems especially robust in detecting disease characterized by high ECV, such as amyloid (in which the ECV is often >0.5) (11) or marked native T<sub>1</sub> contrast diseases such as Anderson-Fabry disease (in which fat storage makes native T<sub>1</sub> fall) (12).

The field of T<sub>1</sub> mapping and noninvasive fibrosis quantification faces the same challenges as any other new technology. A key task will be to let the energy and creative chaos of early development and competing methodologies (e.g., different scanner manufacturers, contrast agents, field strengths, T<sub>1</sub> mapping sequences) transition through collaboration into more standardized methodologies sufficient for use to: diagnose disease; define mechanistic pathways of disease affecting the interstitium, the myocyte, or both; change therapy; and use ECV as a surrogate endpoint in trials of drug development, an aim underpinning the recently formed T<sub>1</sub> mapping development group.

Ultimately, ECV diffuse fibrosis measures could dramatically affect cardiology. We can now dichotomize the myocardium into its cellular and interstitial components, and advance understanding of disease mechanisms and their relative contribution to cardiac vulnerability, which are critically important issues. More data demonstrating fibrosis as a therapeutic target are needed, but because fibrosis guides research and patient management in liver and lung disease, the same principles may apply to the heart. Conceivably, T<sub>1</sub> mapping for ECV could facilitate drug development and guide therapy, especially in the setting of heart failure, in which drug development strategies have produced few positive results over the last decade (13). Exciting times are ahead. Cardiac fibrosis promises to be as fundamental as

fibrosis elsewhere. Its measurement may define disease, predict outcome, determine the choice and timing of interventions, enhance drug development, and be more treatable.

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